

# Event-related fMRI (er-fMRI)

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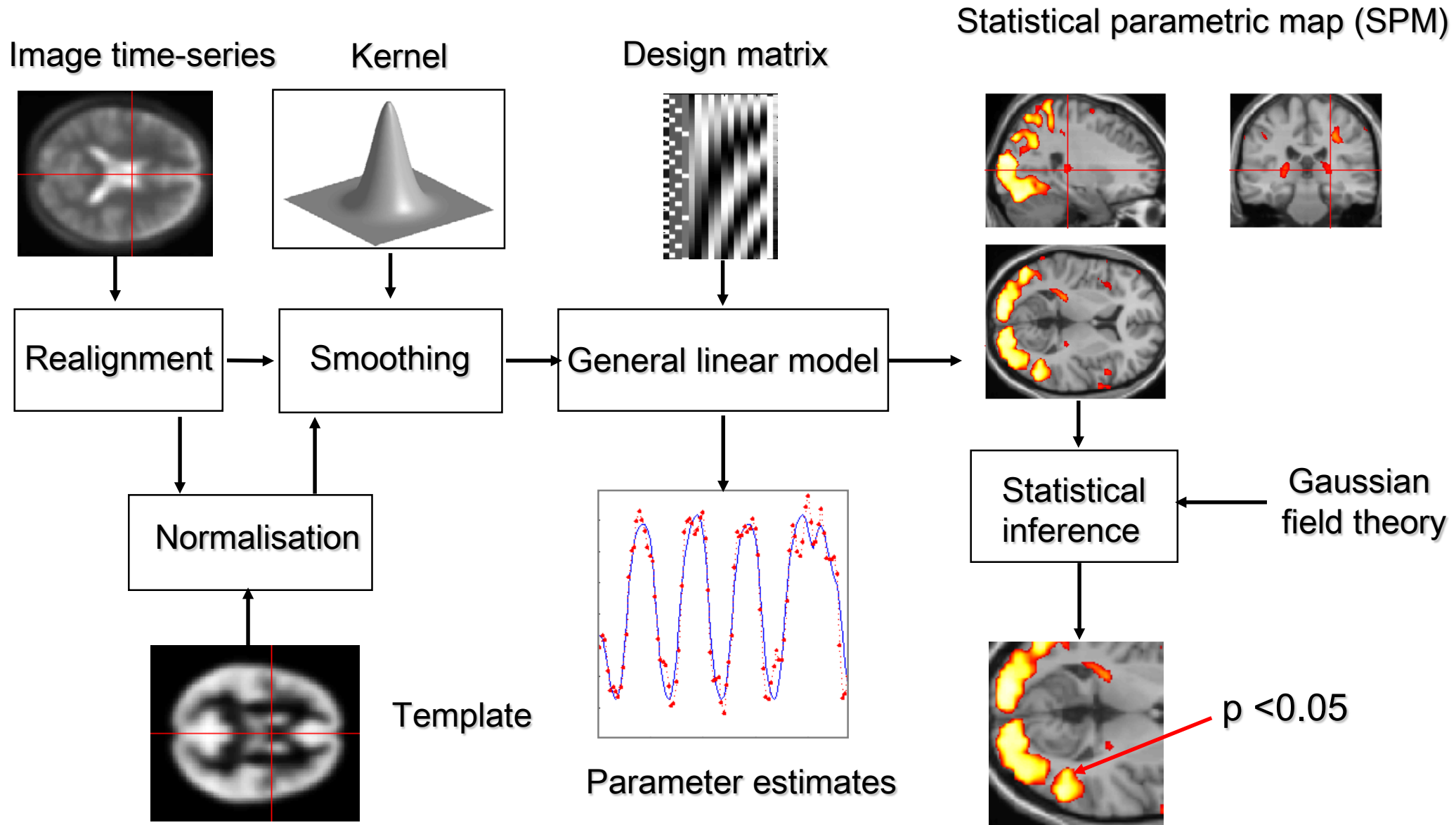
**With many thanks for slides & images to:**

FIL Methods group, particularly Rik Henson and Christian Ruff

Methods & Models for fMRI Data Analysis

06.11.2015

# Overview of SPM



# Overview

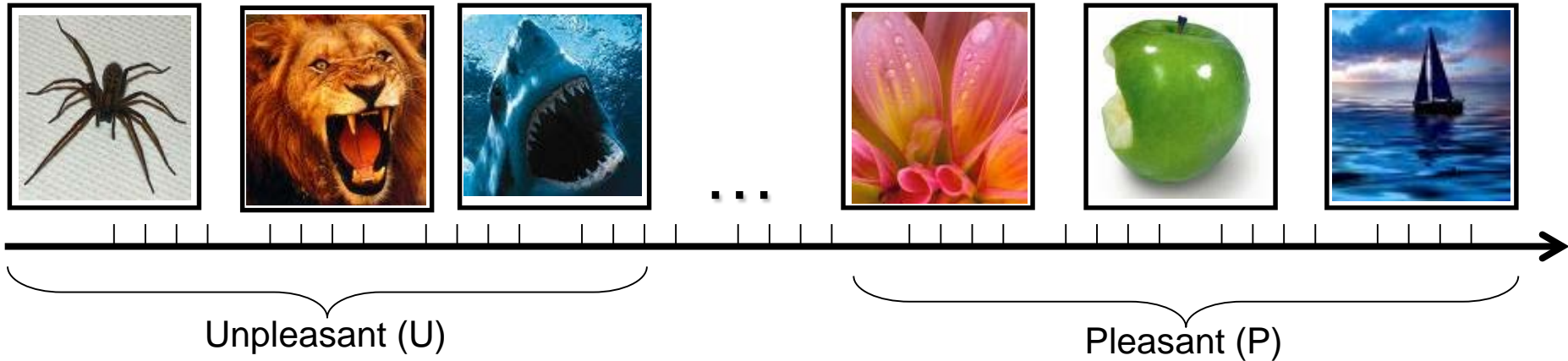
1. Advantages of er-fMRI
2. BOLD impulse response
3. General Linear Model
4. Temporal basis functions
5. Timing issues
6. Design optimisation
7. Nonlinearities at short SOAs

# Advantages of er-fMRI

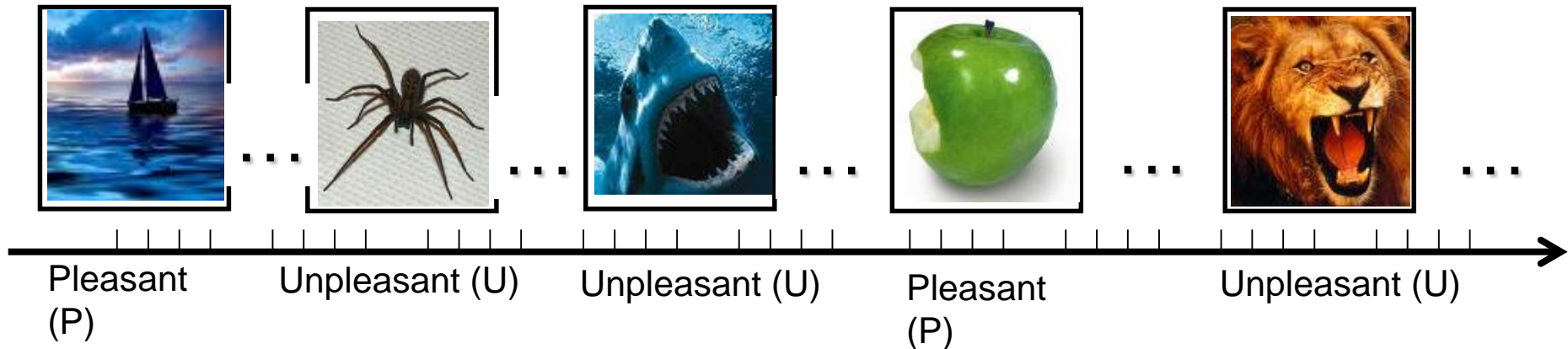
1. Randomised trial order  
c.f. confounds of blocked designs

# er-fMRI: Stimulus randomisation

Blocked designs may trigger expectations and cognitive sets



Intermixed designs can minimise this by stimulus randomisation

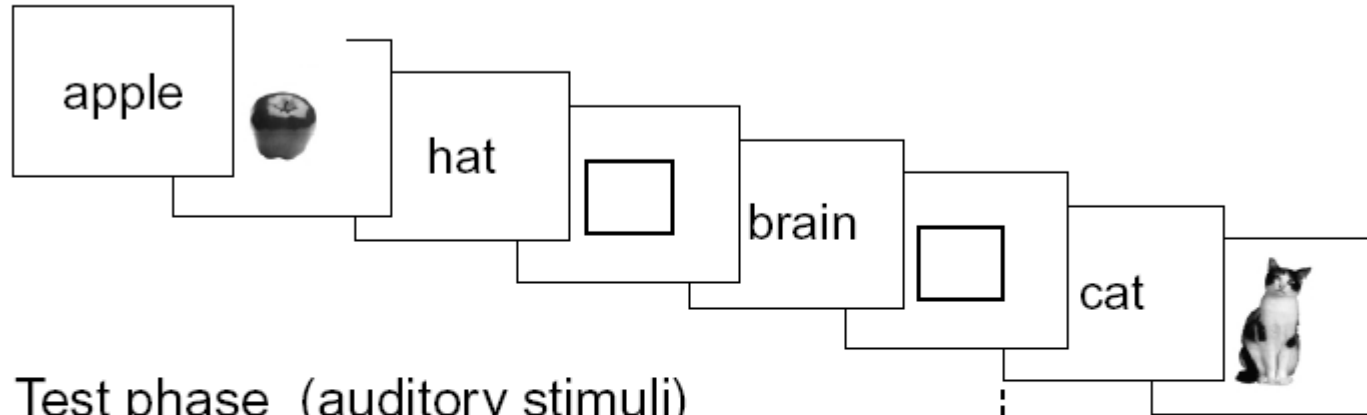


# Advantages of er-fMRI

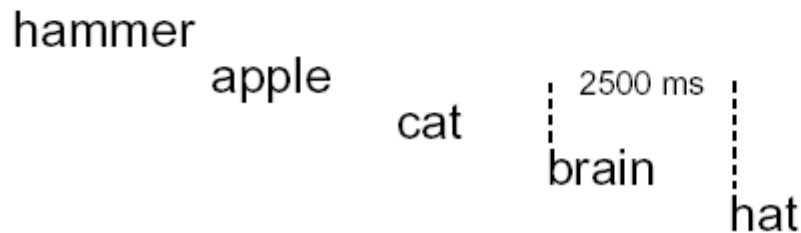
1. Randomised trial order  
c.f. confounds of blocked designs
- 2. Post hoc classification of trials**  
**e.g. according to performance or subsequent memory**

# er-fMRI: post-hoc classification of trials

Study phase (visual stimuli)



Test phase (auditory stimuli)



Participant response:

„was *not* shown as picture“

„was shown as picture“

➔ Items with wrong memory of picture („hat“) were associated with more occipital activity *at encoding* than items with correct rejection („brain“)

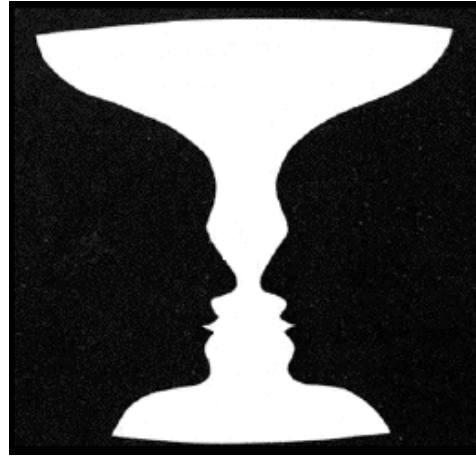
# Advantages of er-fMRI

1. Randomised trial order  
c.f. confounds of blocked designs
2. Post hoc classification of trials  
e.g. according to performance or subsequent memory
3. **Some events can only be indicated by the subject**  
**e.g. spontaneous perceptual changes**

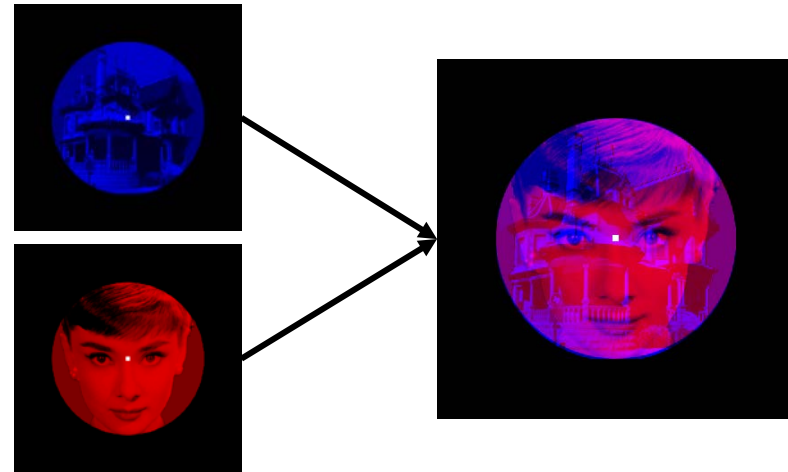


# eFMRI: “on-line” event-definition

Bistable percepts



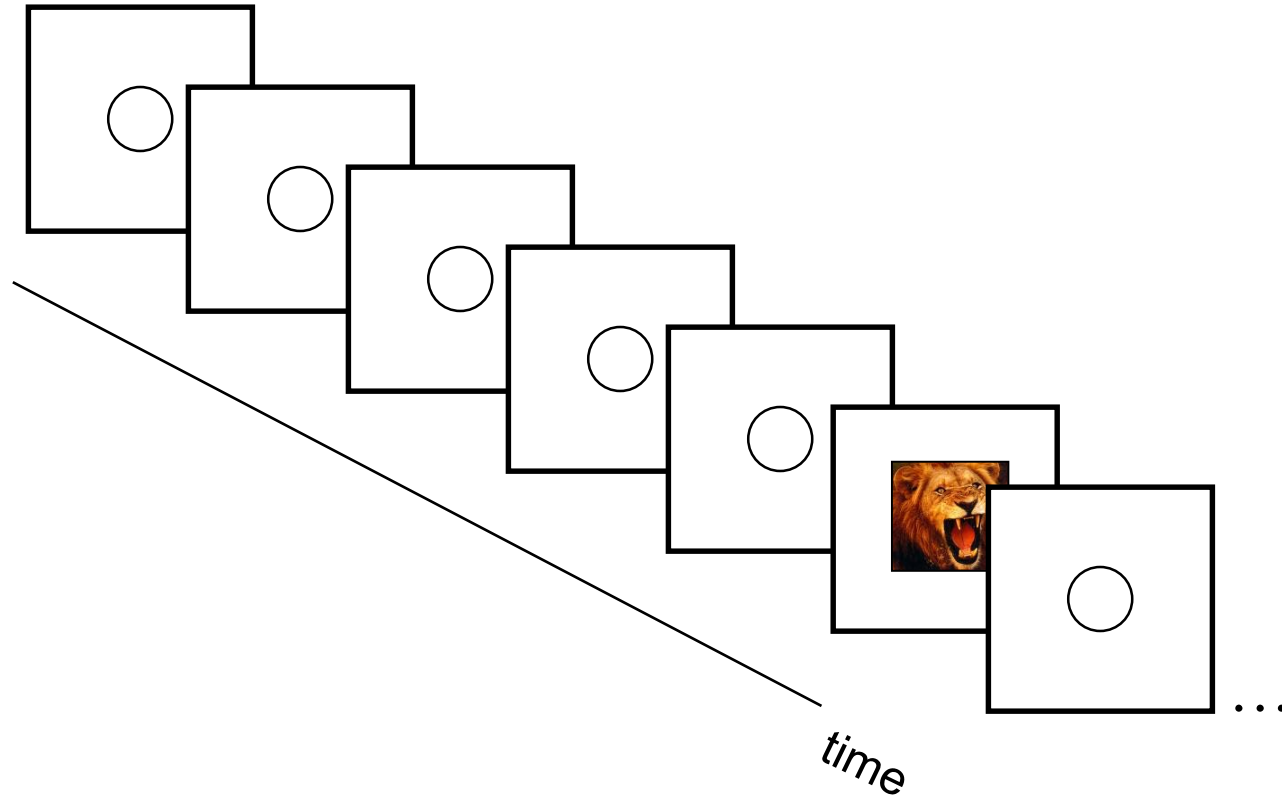
Binocular rivalry



# Advantages of er-fMRI

1. Randomised trial order  
c.f. confounds of blocked designs
2. Post hoc classification of trials  
e.g. according to performance or subsequent memory
3. Some events can only be indicated by the subject  
e.g. spontaneous perceptual changes
4. **Some trials cannot be blocked**  
e.g. “oddball” designs

# er-fMRI: “oddball” designs

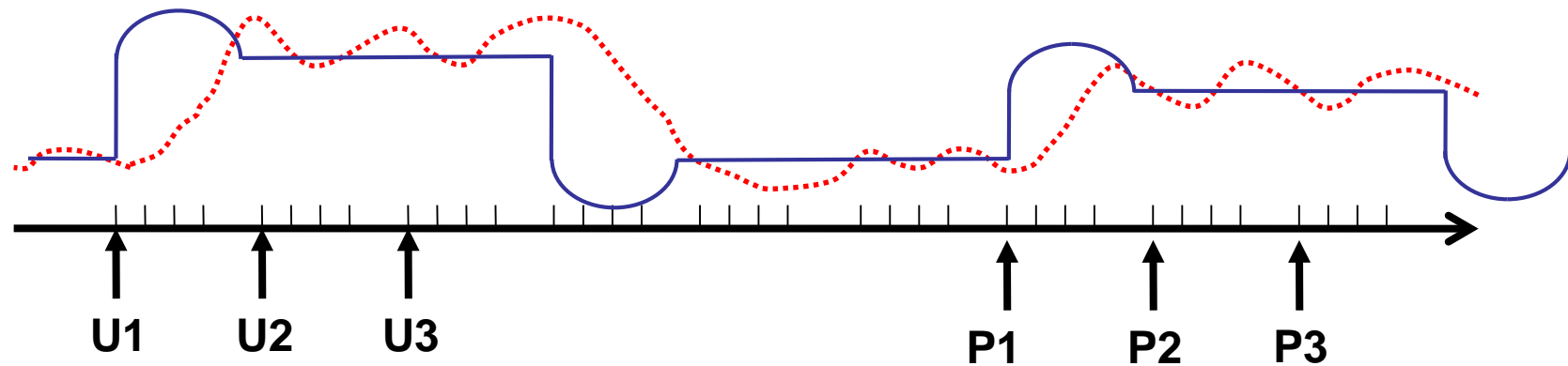


# Advantages of er-fMRI

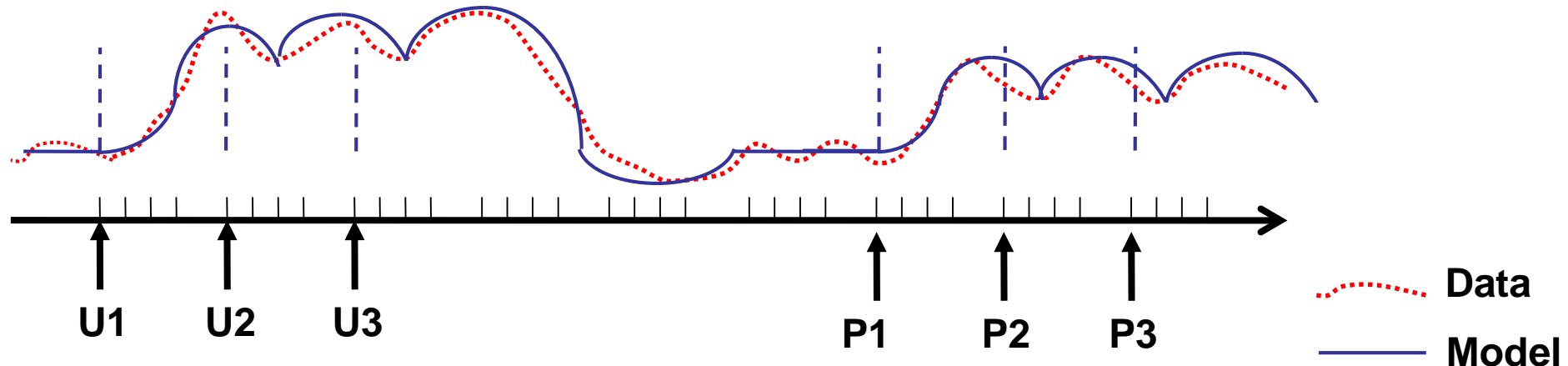
1. Randomised trial order  
c.f. confounds of blocked designs
2. Post hoc classification of trials  
e.g. according to performance or subsequent memory
3. Some events can only be indicated by subject  
e.g. spontaneous perceptual changes
4. Some trials cannot be blocked  
e.g. “oddball” designs
5. **More accurate models even for blocked designs?**  
**“state-item” interactions**

# er-fMRI: “event-based” model of block-designs

“Epoch” model assumes constant neural processes throughout block

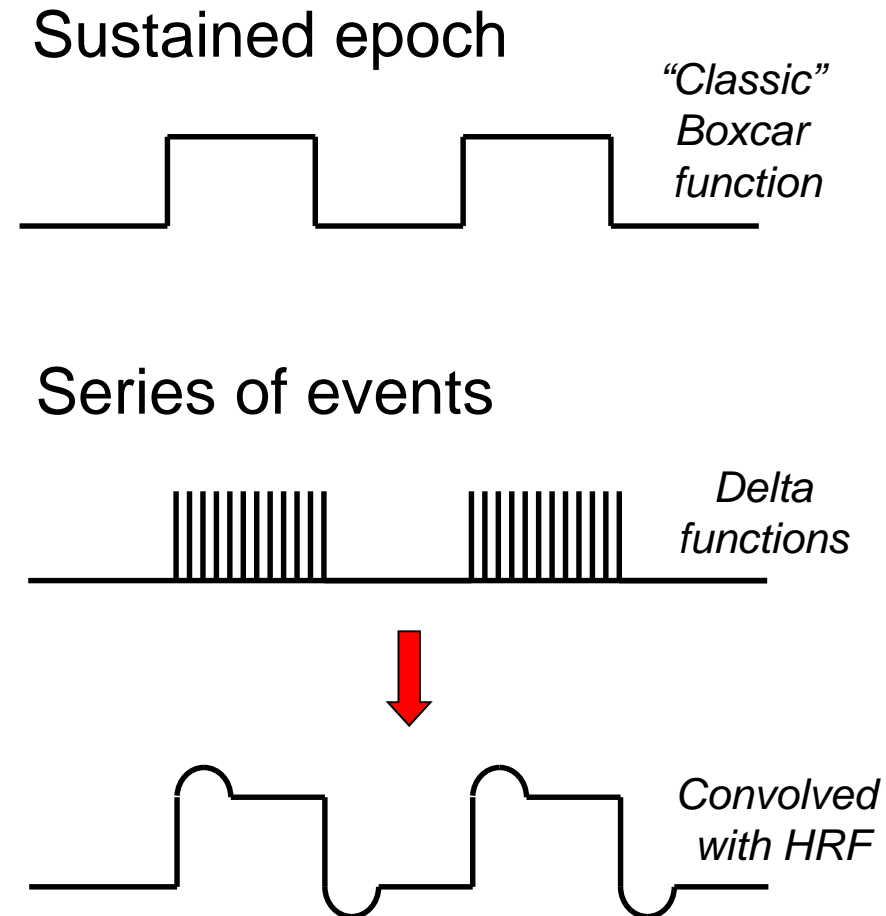


“Event” model may capture state-item interactions



# Modeling block designs: epochs vs events

- *Designs* can be blocked or intermixed, BUT *models* for blocked designs can be epoch- or event-related
- Epochs are periods of sustained stimulation (e.g, box-car functions)
- Events are impulses (delta-functions)
- Near-identical regressors can be created by 1) sustained epochs, 2) rapid series of events (SOAs < ~3s)
- In SPM, all conditions are specified in terms of their 1) onsets and 2) durations
  - ... epochs: variable or constant duration
  - ... events: zero duration

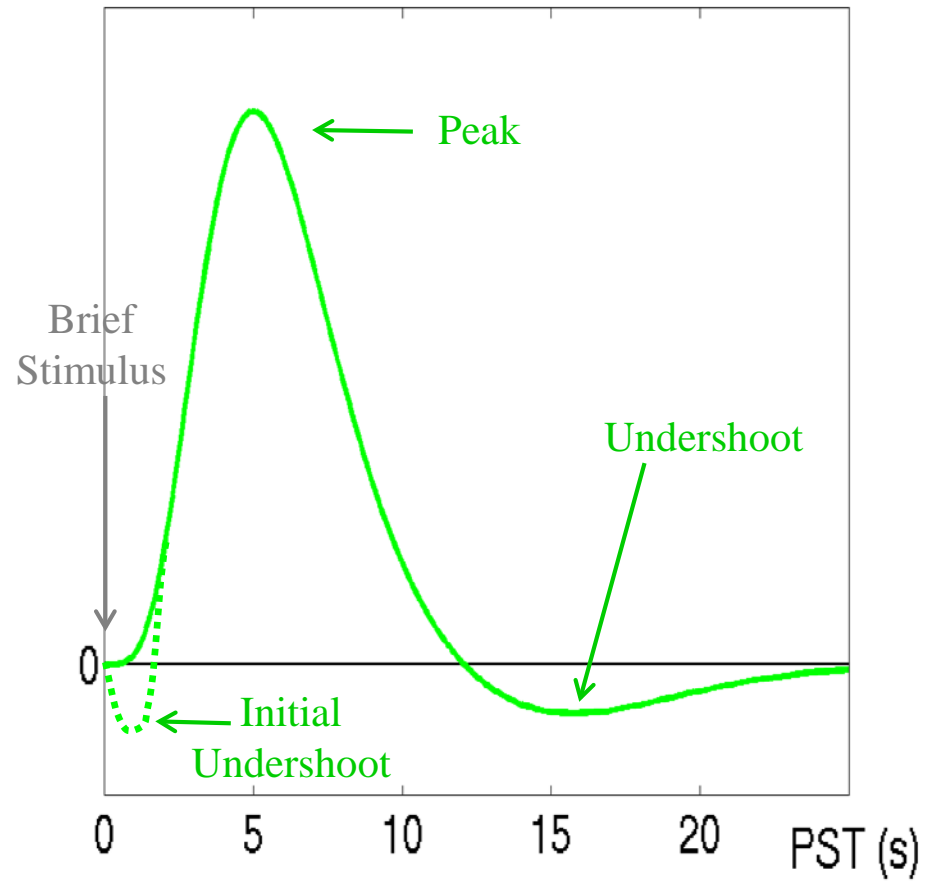


# Disadvantages of er-fMRI

1. Less efficient for detecting effects than blocked designs.
2. Some psychological processes may be better blocked (e.g. task-switching, attentional instructions).

# BOLD impulse response

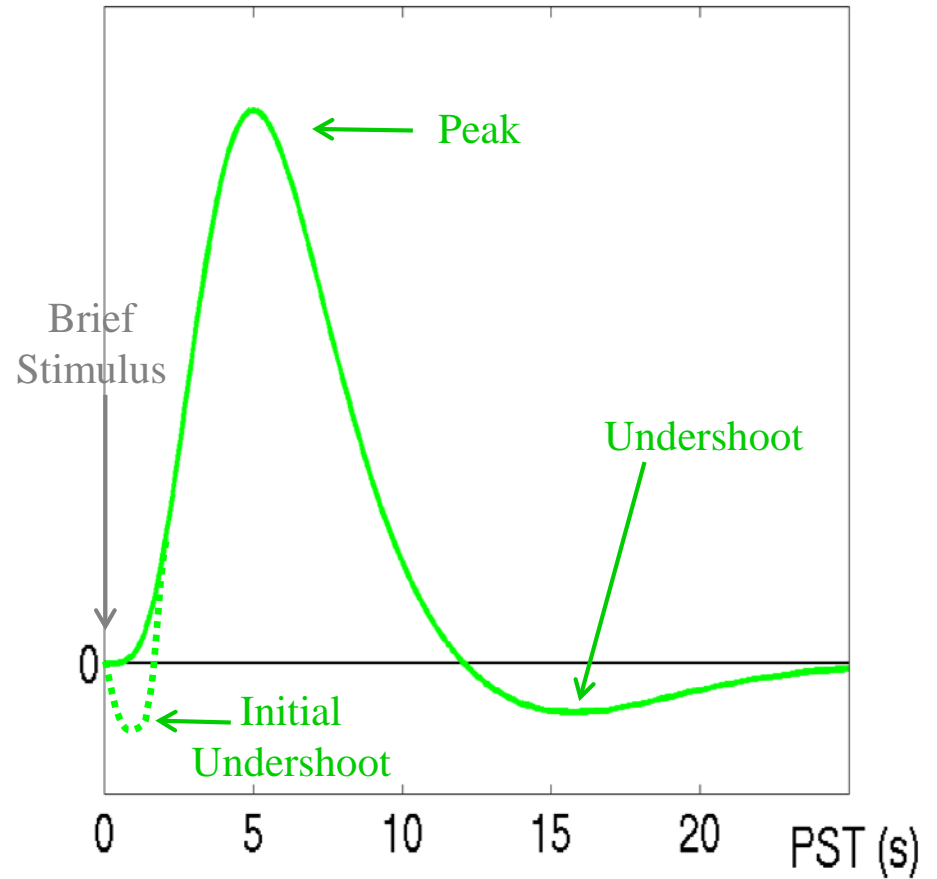
- Function of blood volume and deoxyhemoglobin content (Buxton et al. 1998)
- Peak (max. oxygenation) 4-6s post-stimulus; return to baseline after 20-30s
- initial undershoot sometimes observed (Malonek & Grinvald, 1996)
- Similar across V1, A1, S1...
- ... but differences across other regions (Schacter et al. 1997) and individuals (Aguirre et al. 1998)





# BOLD impulse response

- Early er-fMRI studies used a long Stimulus Onset Asynchrony (SOA) to allow BOLD response to return to baseline.
- However, if the BOLD response is explicitly modelled, overlap between successive responses at short SOAs can be accommodated...
- ... particularly if responses are assumed to superpose linearly.
- Short SOAs can give a more efficient design (see below).



# General Linear (Convolution) Model

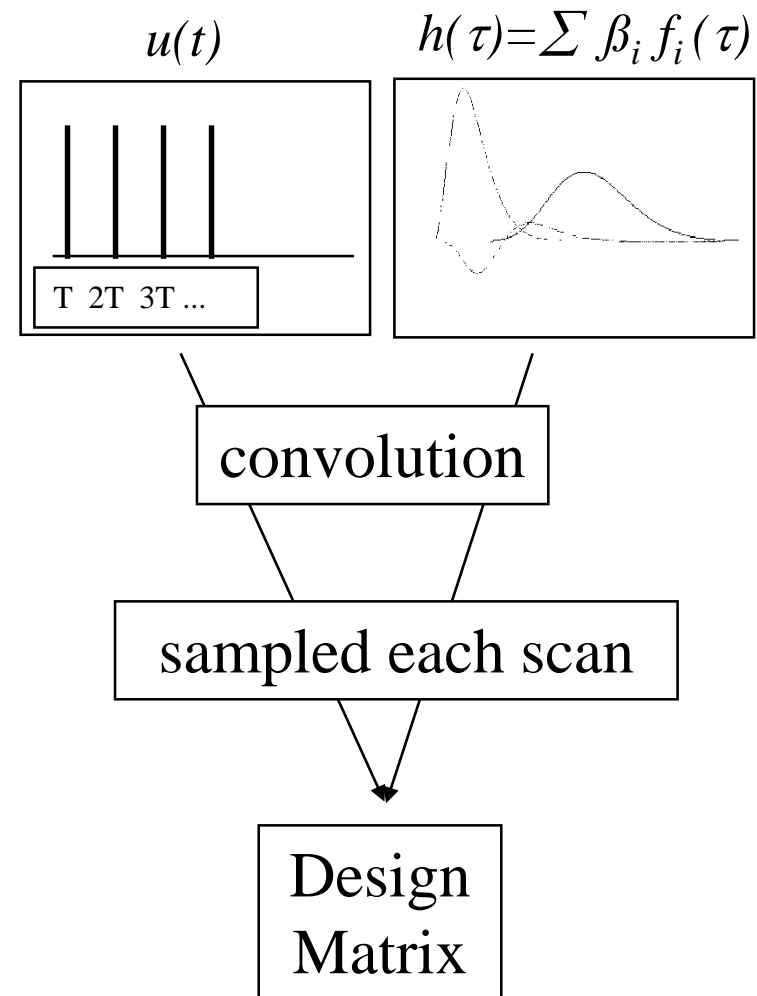
For block designs, the exact shape of the convolution kernel (i.e. HRF) does not matter much.

For event-related designs this becomes much more important.

Usually, we use more than a single basis function to model the HRF.

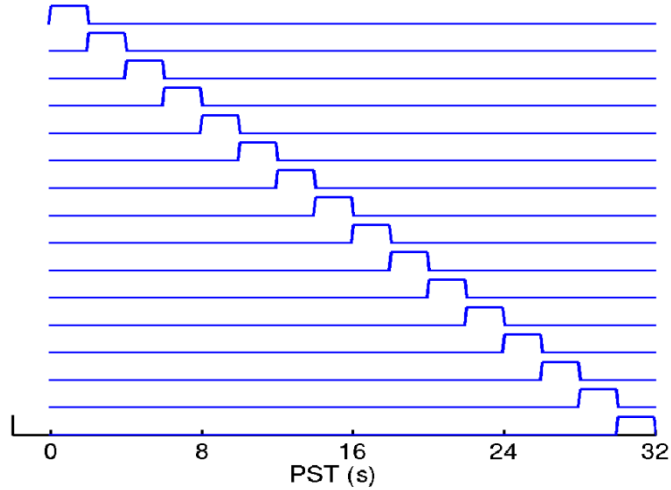
GLM for a single voxel:

$$\mathbf{y}(\mathbf{t}) = \mathbf{u}(\mathbf{t}) \otimes \mathbf{h}(\boldsymbol{\tau}) + \boldsymbol{\varepsilon}(\mathbf{t})$$

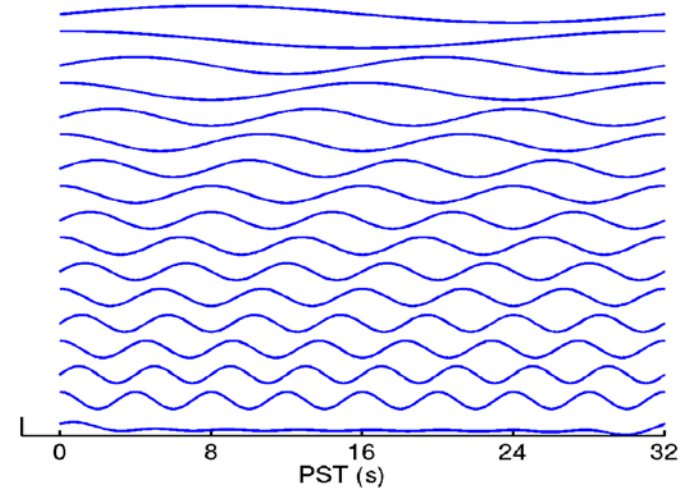


# Temporal basis functions

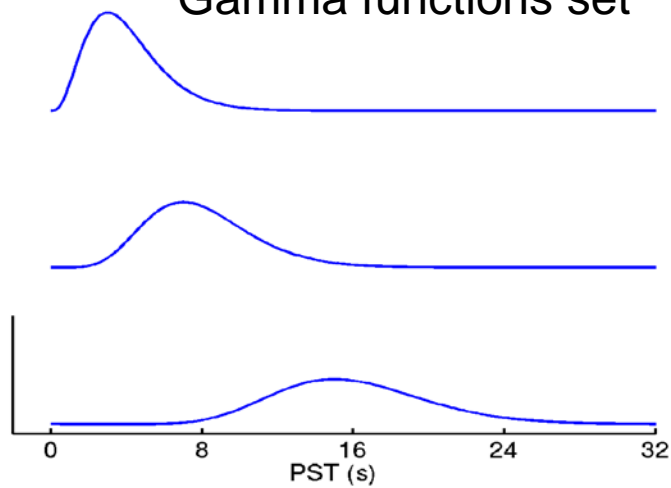
Finite Impulse Response (FIR) model



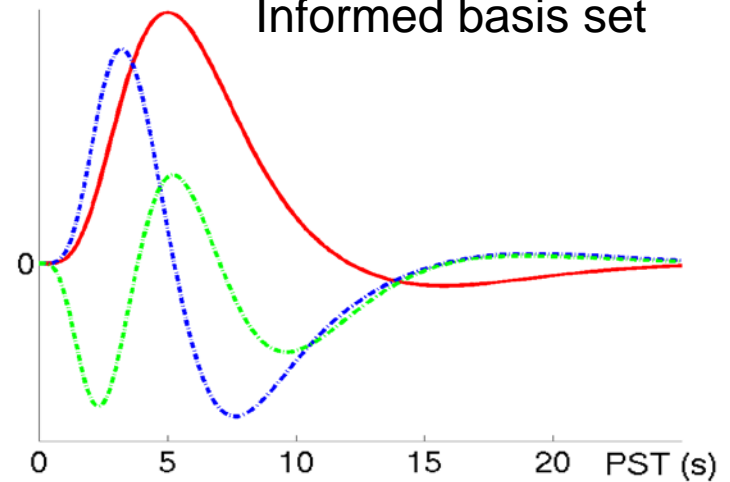
Fourier basis set



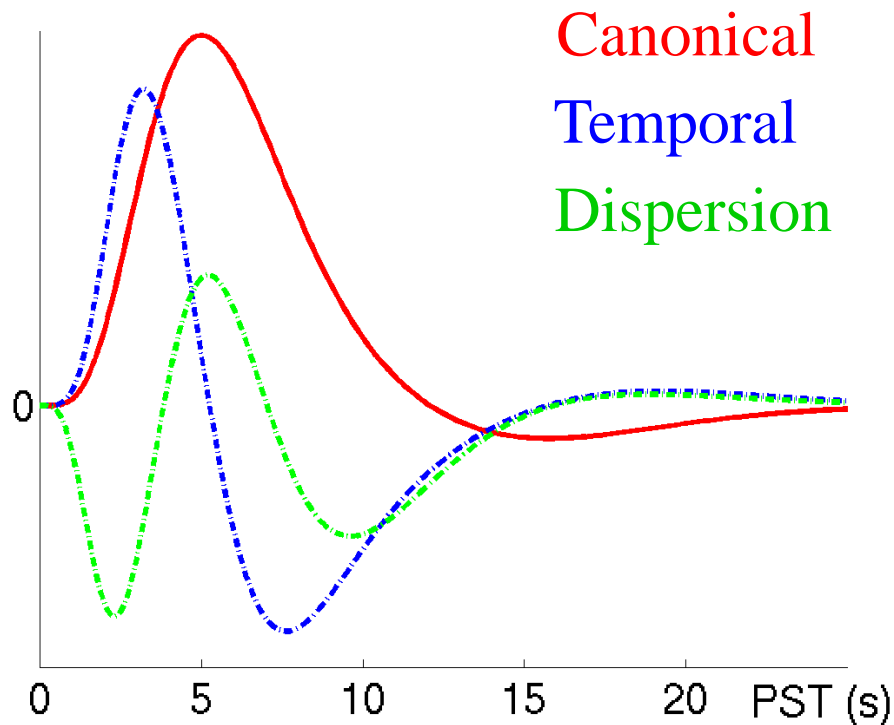
Gamma functions set



Informed basis set



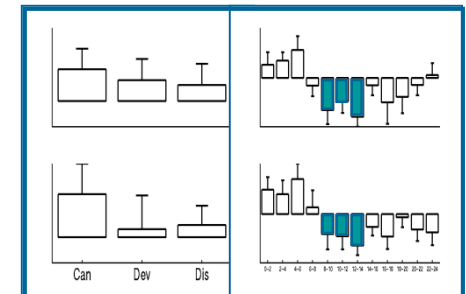
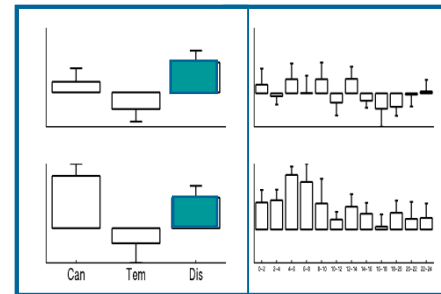
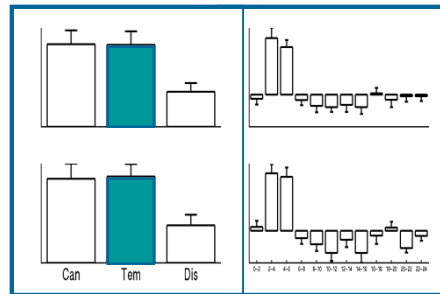
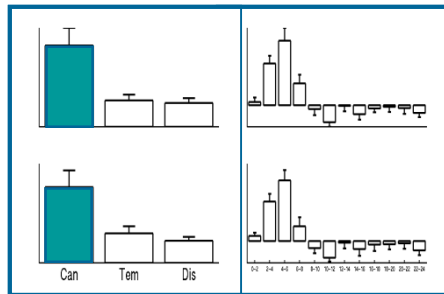
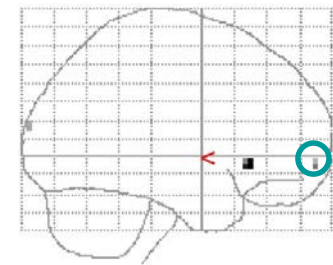
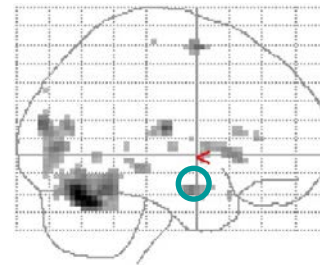
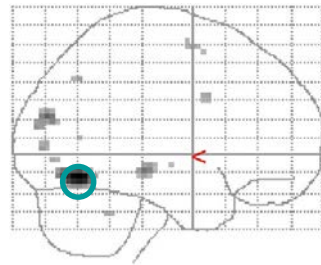
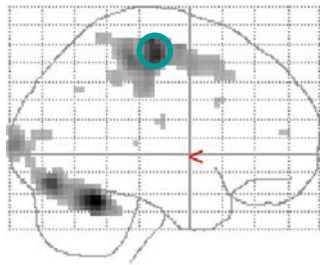
# Informed basis set



- Canonical HRF (2 gamma functions)  
*plus* Multivariate Taylor expansion in:  
time (*Temporal Derivative*)  
width (*Dispersion Derivative*)
- F-tests allow testing for any responses of any shape.
- T-tests on canonical HRF alone (at 1<sup>st</sup> level) can be improved by derivatives reducing residual error, and can be interpreted as “amplitude” differences, assuming canonical HRF is a reasonable fit.

# Temporal basis sets: Which one?

In this example (rapid motor response to faces, *Henson et al, 2001*)...



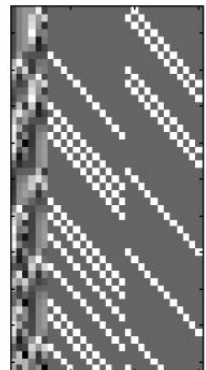
**Canonical**

**+ Temporal**

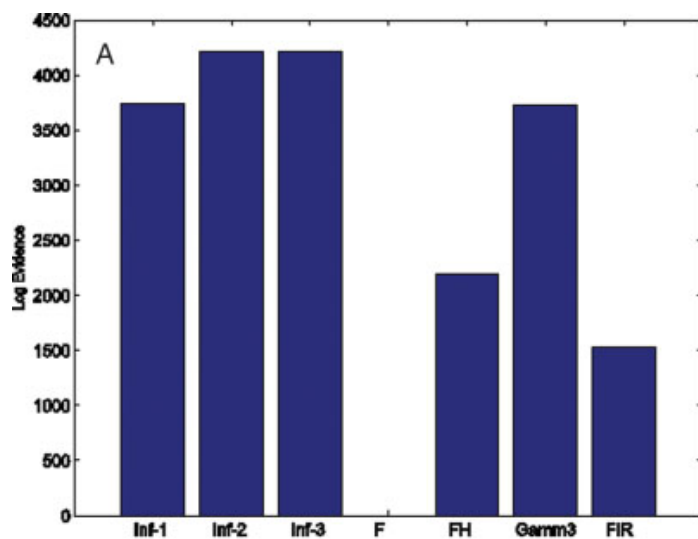
**+ Dispersion**

**+ FIR**

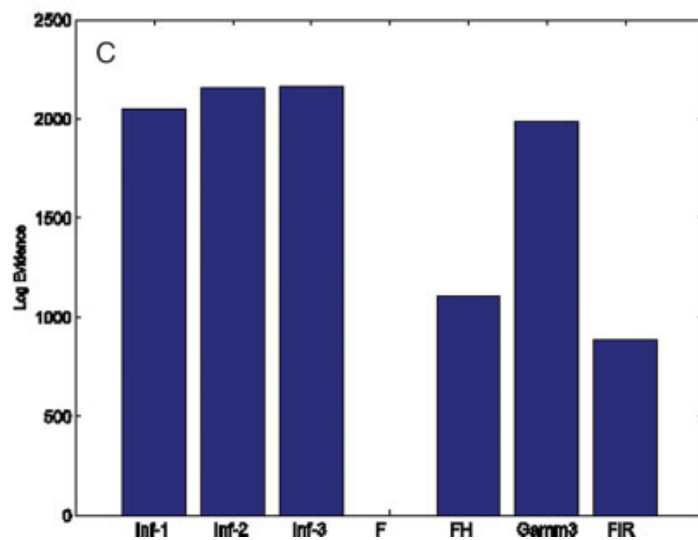
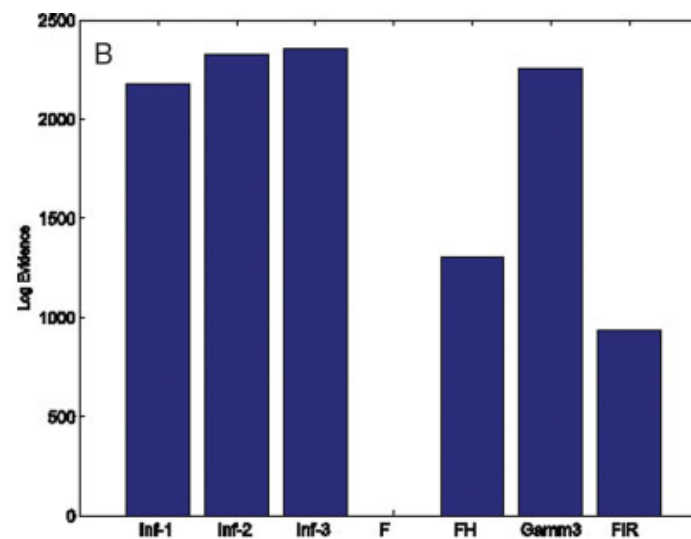
- canonical + temporal + dispersion derivatives appear sufficient
- may not be for more complex trials (e.g. stimulus-delay-response)
- but then such trials better modelled with separate neural components (i.e. activity no longer delta function) (Zarahn, 1999)



left occipital cortex

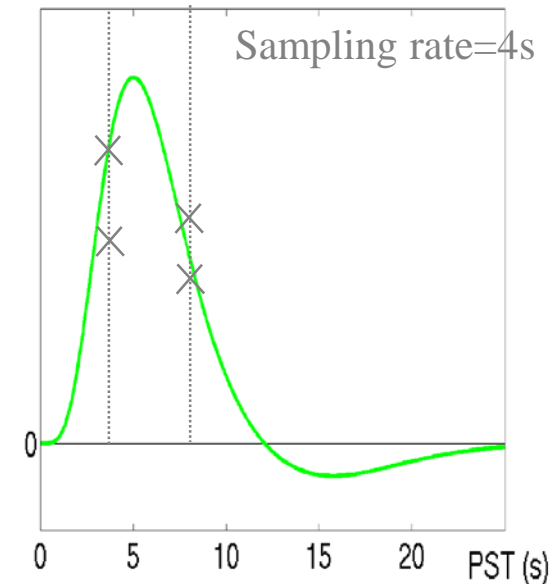
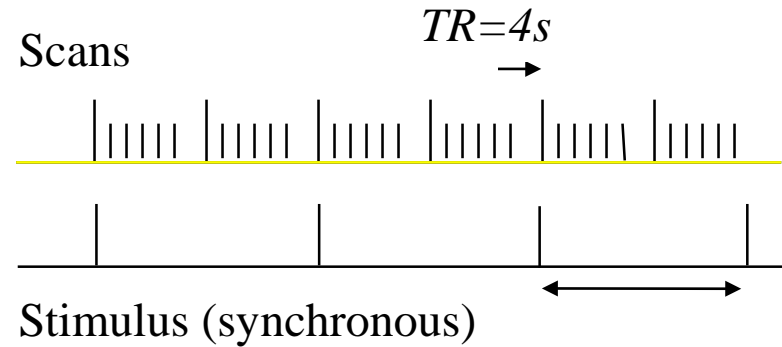


right occipital cortex



# Timing Issues : Practical

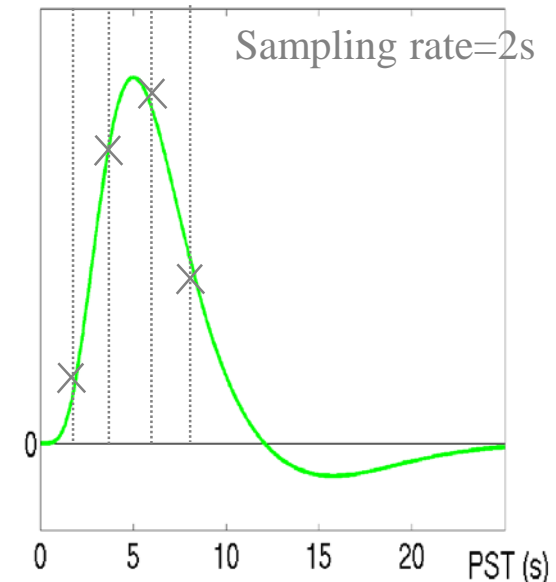
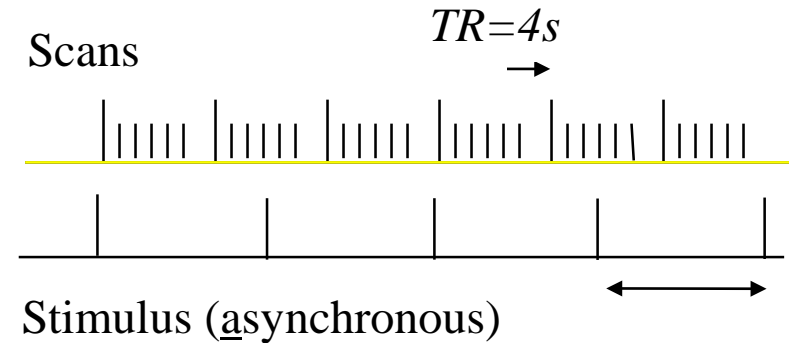
- Assume TR is 4s
- Sampling at [0,4,8,12...] post- stimulus may miss peak signal



SOA = Stimulus onset asynchrony  
(= time between onsets of two subsequent stimuli)

# Timing Issues : Practical

- Assume TR is 4s
- Sampling at [0,4,8,12...] post- stimulus may miss peak signal
- Higher effective sampling by:
  - 1. Asynchrony, e.g.  $SOA = 1.5 \times TR$



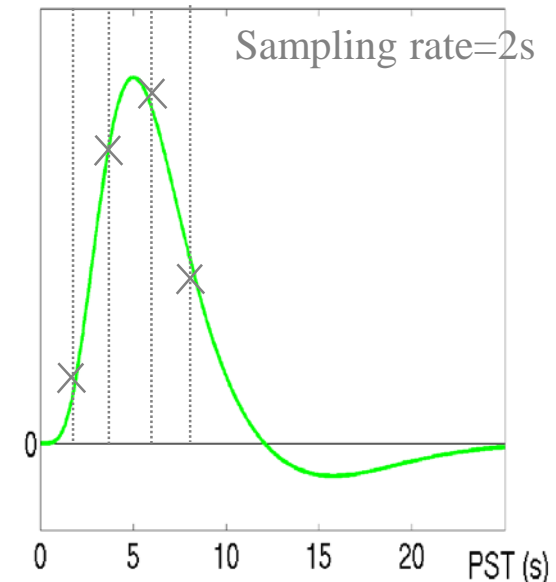
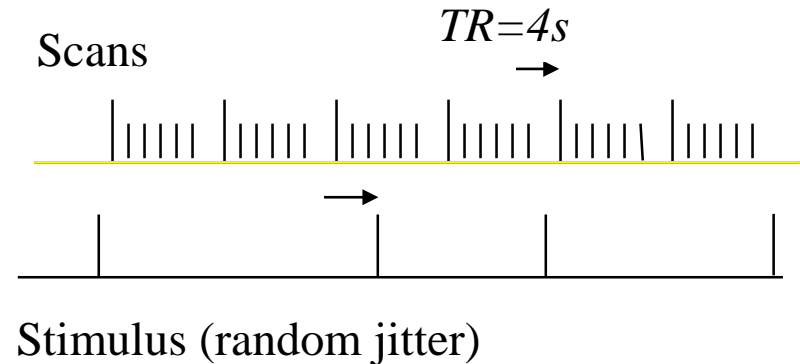
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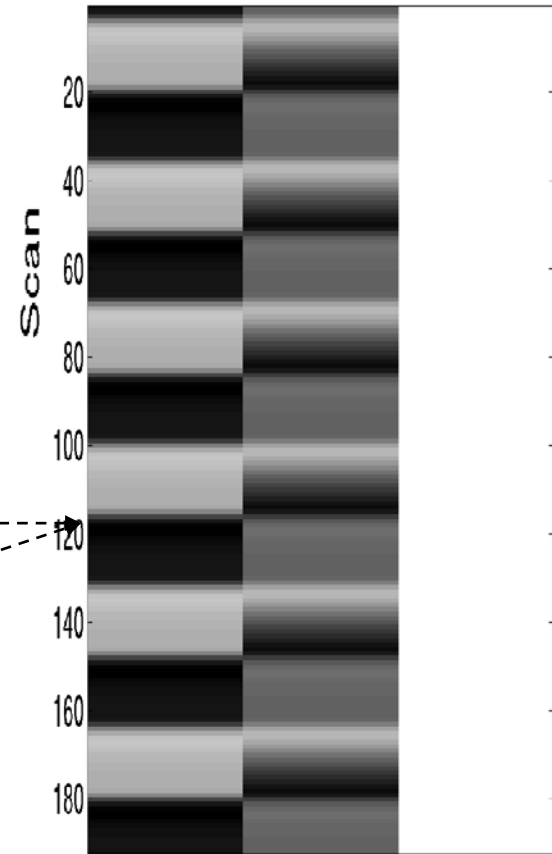
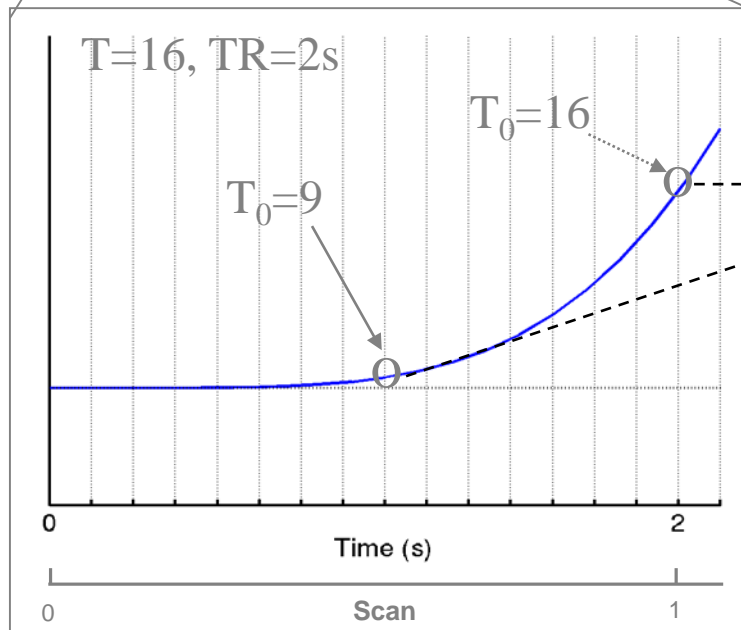
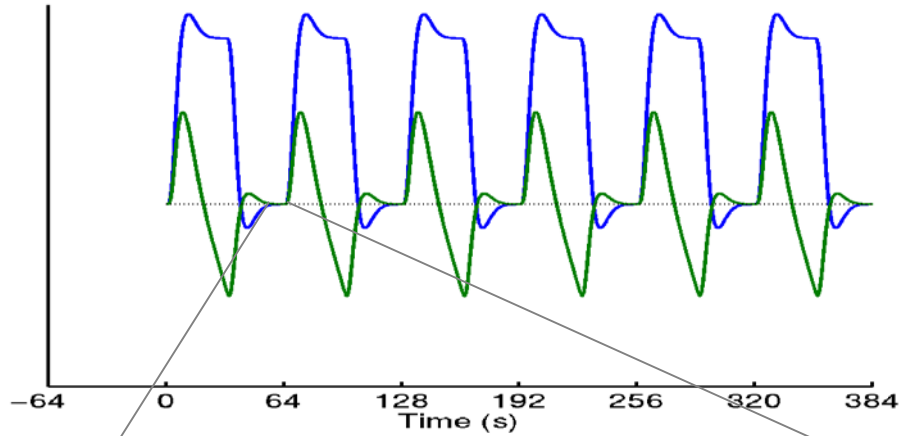
# Timing Issues : Practical

- Assume TR is 4s
- Sampling at [0,4,8,12...] post- stimulus may miss peak signal
- Higher effective sampling by:
  - 1. Asynchrony, e.g.  $SOA = 1.5 \times TR$
  - 2. Random jitter, e.g.  $SOA = (2 \pm 0.5) \times TR$
- Better response characterisation (Miezin et al, 2000)

SOA = Stimulus onset asynchrony  
(= time between onsets of two subsequent stimuli)

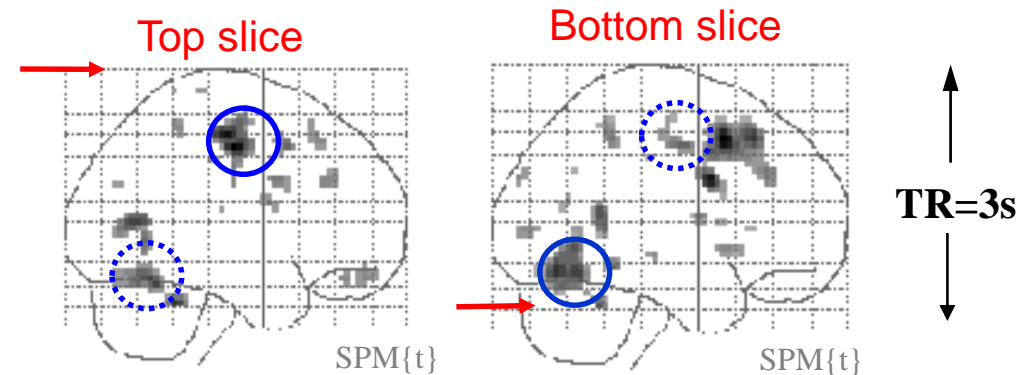


# Slice-timing



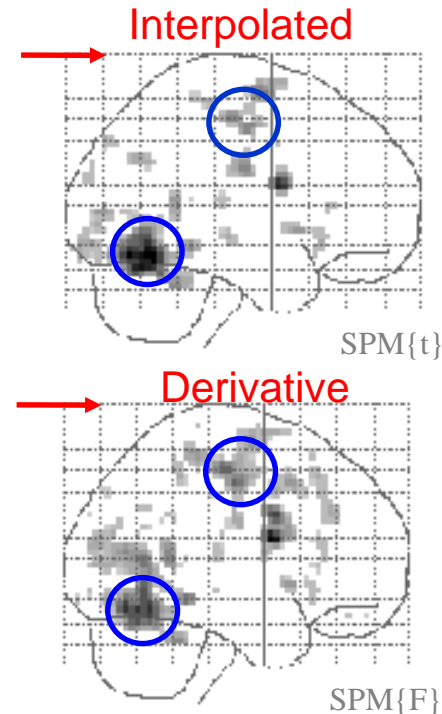
# Slice-timing

- Slices acquired at different times, yet model is the same for all slices  
=> *different results (using canonical HRF) for different reference slices*



- Solutions:

1. Temporal interpolation of data  
... but less good for longer TRs
2. More general basis set (e.g. with temporal derivatives)  
... but more complicated design matrix



# Design efficiency

- The aim is to minimize the standard error of a  $t$ -contrast (i.e. the denominator of a  $t$ -statistic).

$$\text{var}(c^T \hat{\beta}) = \hat{\sigma}^2 c^T (X^T X)^{-1} c$$

$$T = \frac{c^T \hat{\beta}}{\sqrt{\text{var}(c^T \hat{\beta})}}$$

- This is equivalent to maximizing the efficiency  $\varepsilon$ :

$$\varepsilon(\hat{\sigma}^2, c, X) = (\hat{\sigma}^2 c^T (X^T X)^{-1} c)^{-1}$$

Noise variance

Design variance

- If we assume that the noise variance is independent of the specific design:

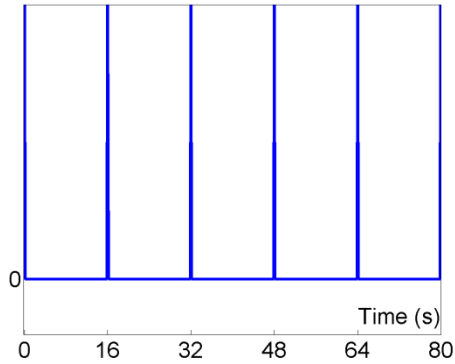
$$\varepsilon(c, X) = (c^T (X^T X)^{-1} c)^{-1}$$

NB: efficiency depends on design matrix and the chosen contrast !

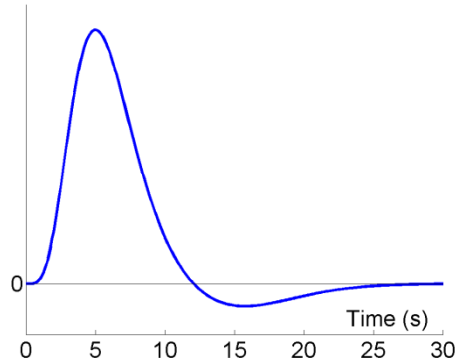
- This is a relative measure: all we can say is that one design is more efficient than another (for a given contrast).

# Fixed SOA = 16s

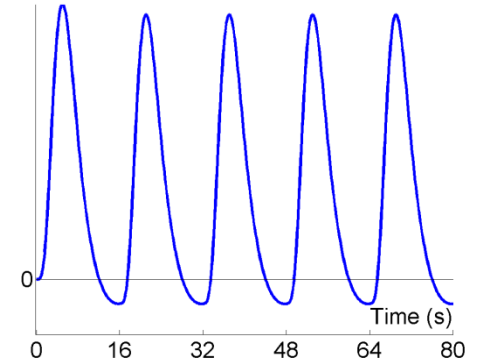
Stimulus ("Neural")



HRF



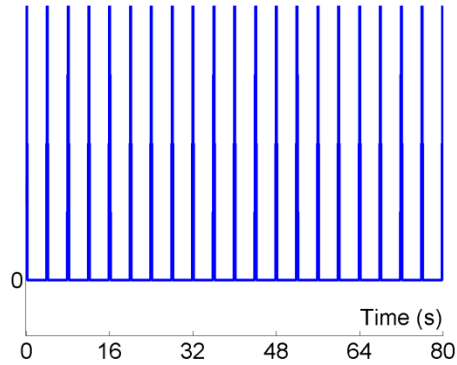
Predicted Data



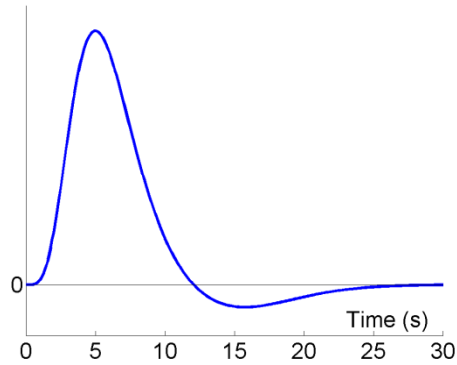
Not particularly efficient...

# Fixed SOA = 4s

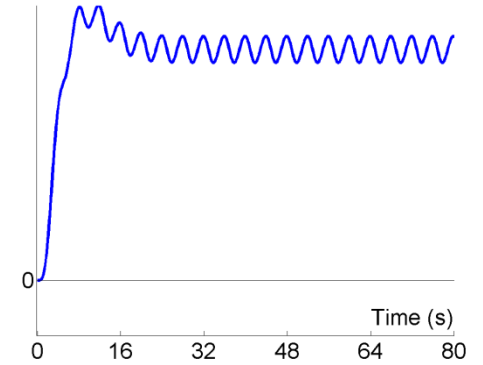
Stimulus ("Neural")



HRF



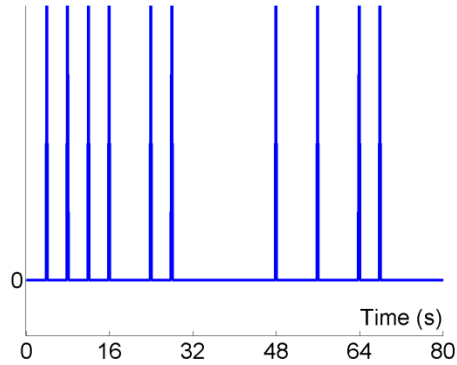
Predicted Data



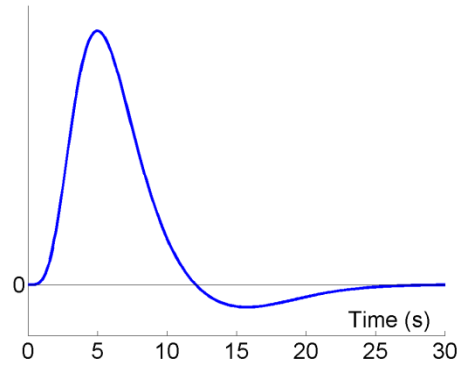
Very inefficient...

# Randomised, $SOA_{\min} = 4s$

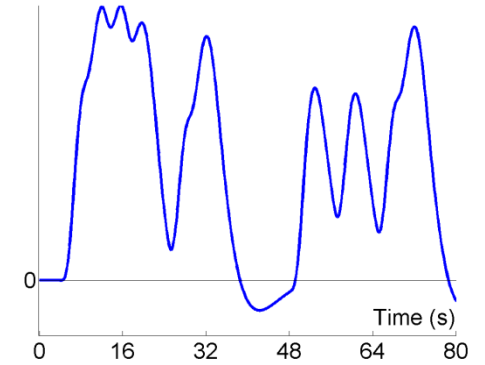
Stimulus ("Neural")



HRF



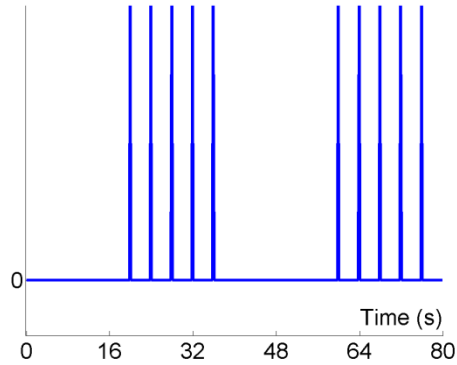
Predicted Data



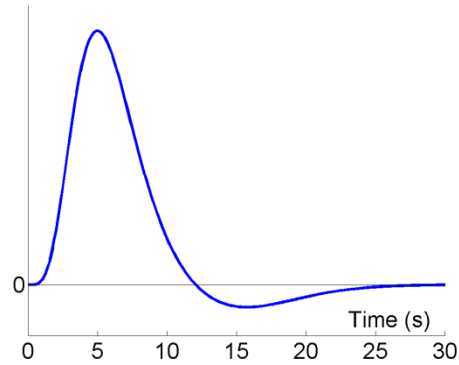
More efficient ...

# Blocked, $SOA_{\min} = 4s$

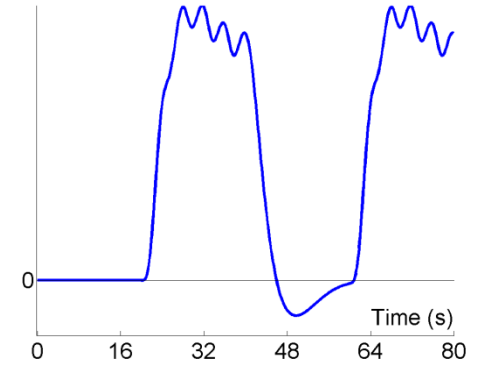
Stimulus ("Neural")



HRF



Predicted Data



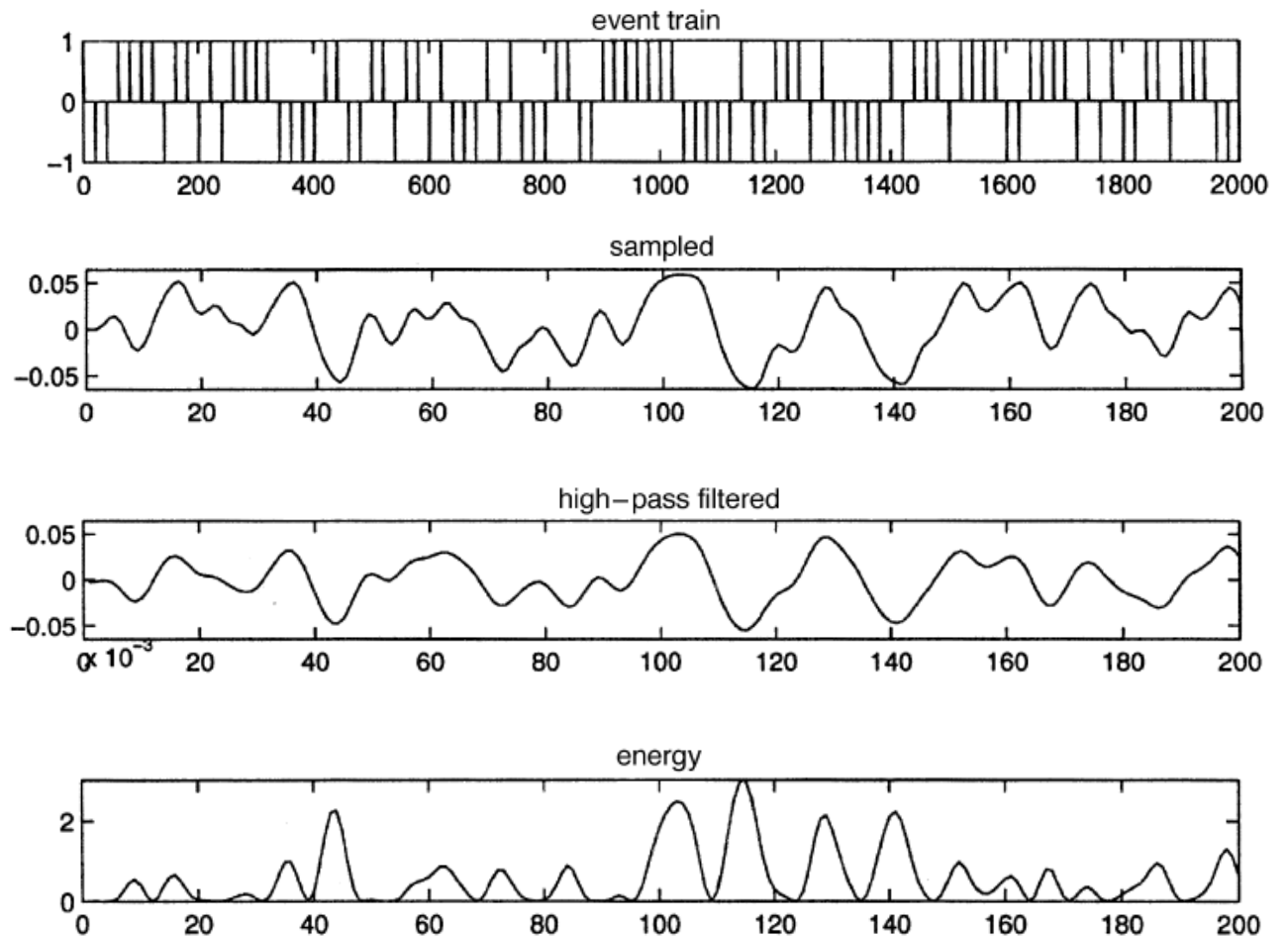
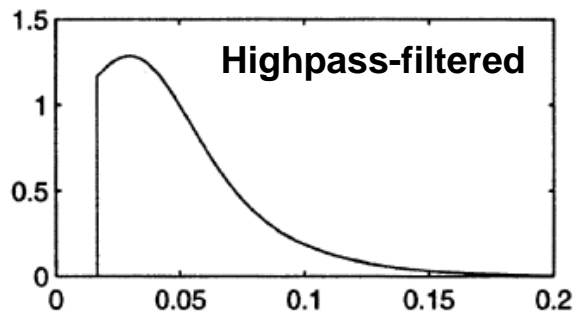
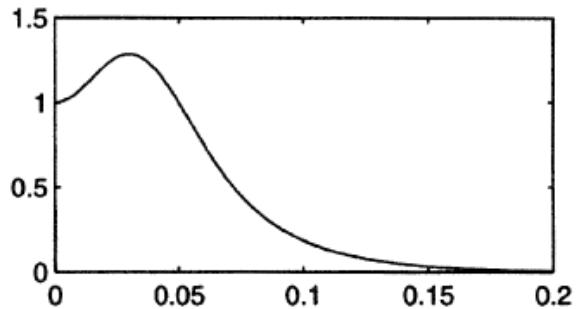
Even more efficient...



# Another perspective on efficiency

## Hemodynamic transfer function

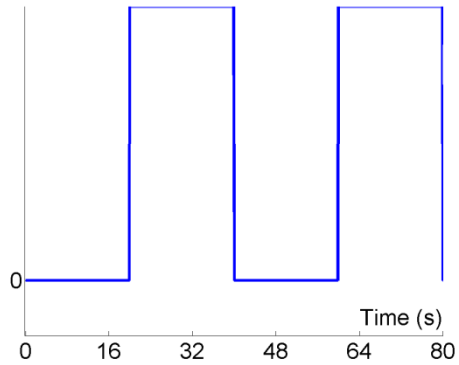
(based on canonical HRF):  
neural activity (Hz)  $\rightarrow$  BOLD



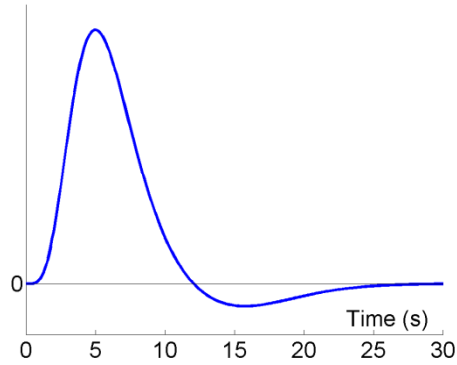
**efficiency = bandpassed signal energy**

# Blocked, epoch = 20s

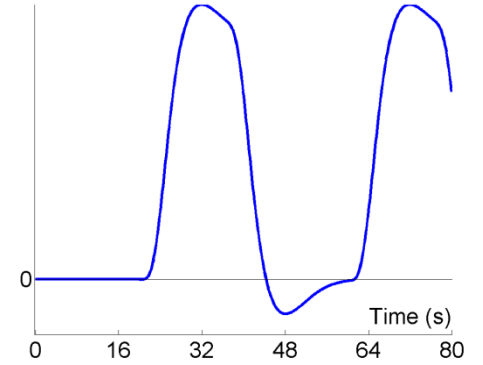
Stimulus ("Neural")



HRF

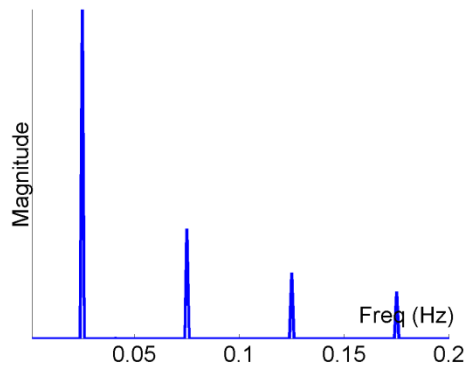


Predicted Data



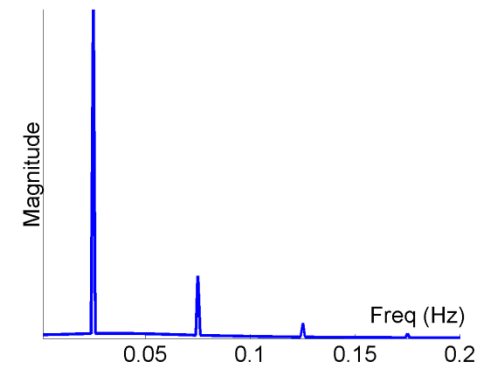
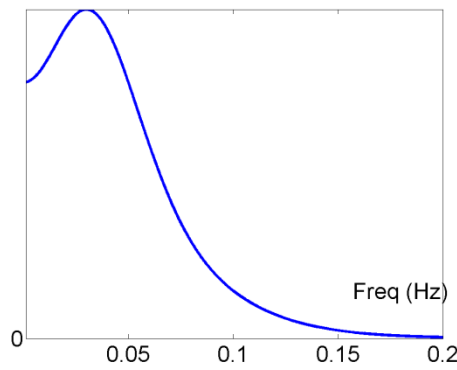
$\otimes$

=



$\times$

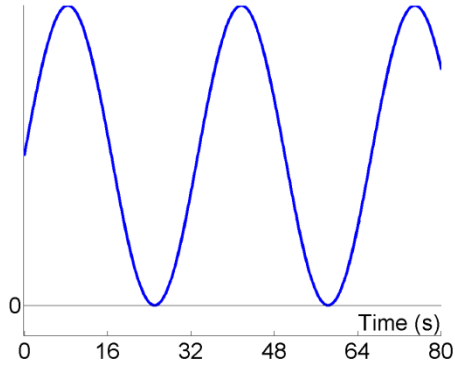
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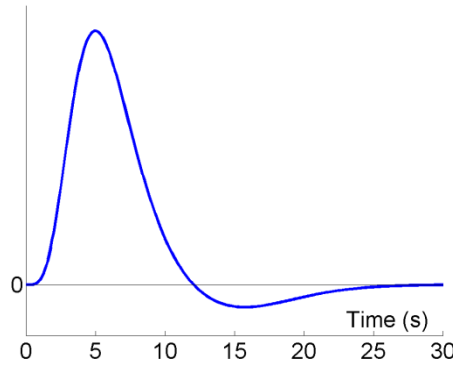
Blocked-epoch (with short SOA)

# Sinusoidal modulation, $f = 1/33\text{s}$

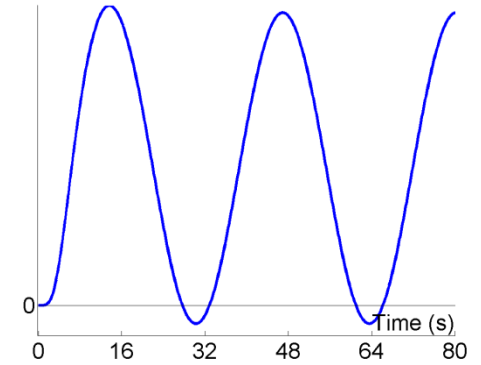
Stimulus ("Neural")



HRF

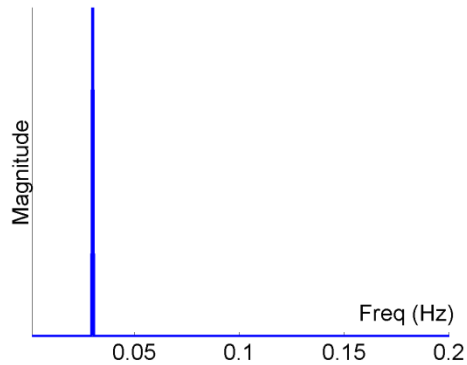


Predicted Data



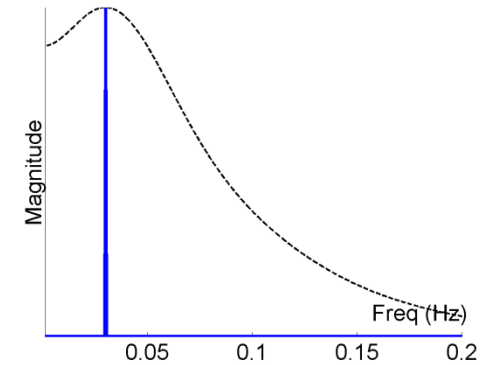
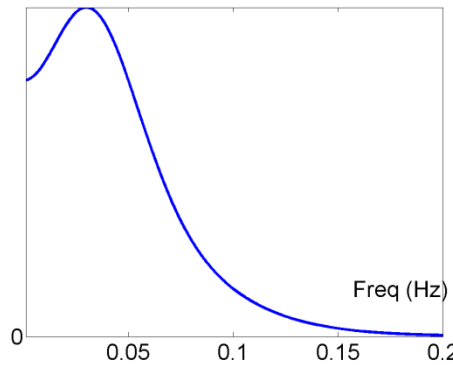
$\otimes$

$=$



$\times$

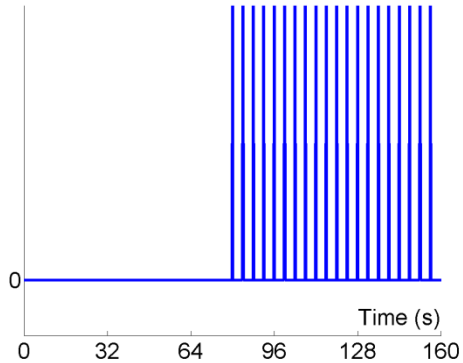
$=$



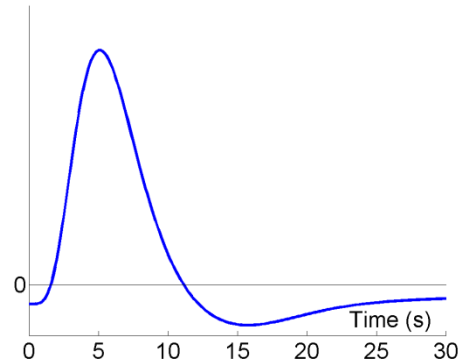
The most efficient design of all!

# Blocked (80s), $SOA_{min}=4s$ , highpass filter = $1/120s$

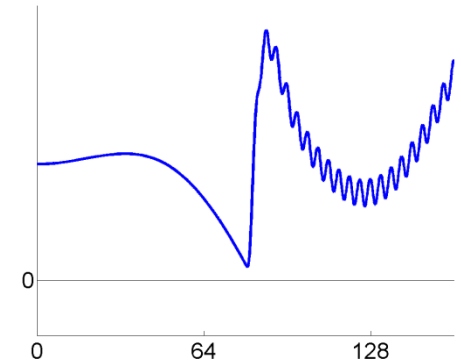
Stimulus ("Neural")



HRF

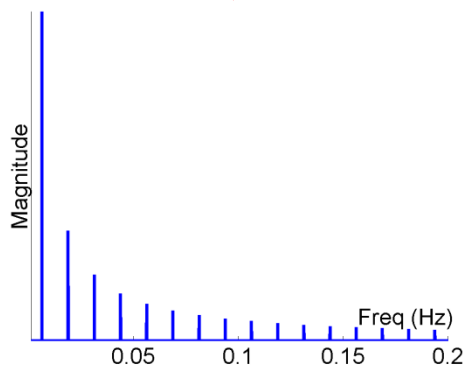


Predicted data  
(incl. HP filtering!)



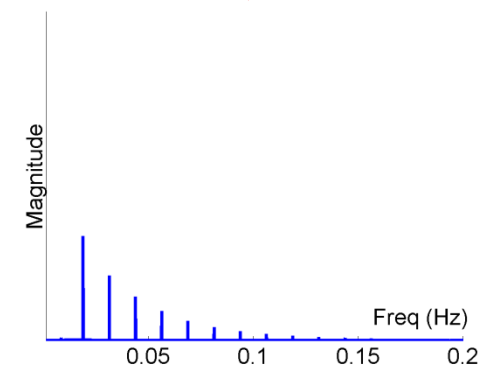
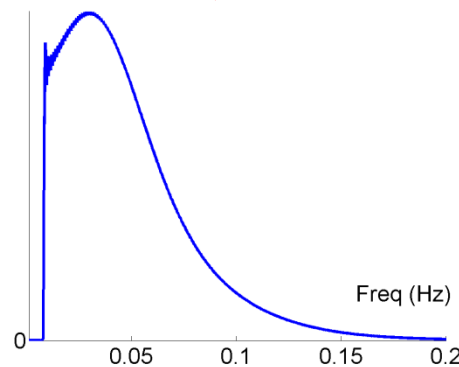
$\otimes$

=



$\times$

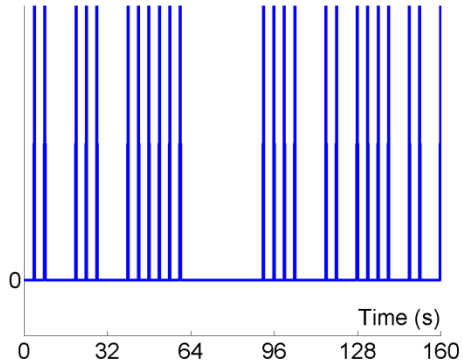
=



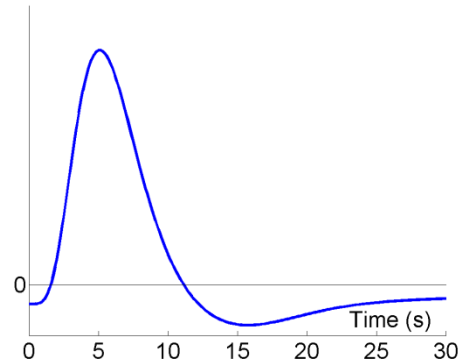
Don't use long (>60s) blocks!

# Randomised, $SOA_{\min}=4s$ , highpass filter = $1/120s$

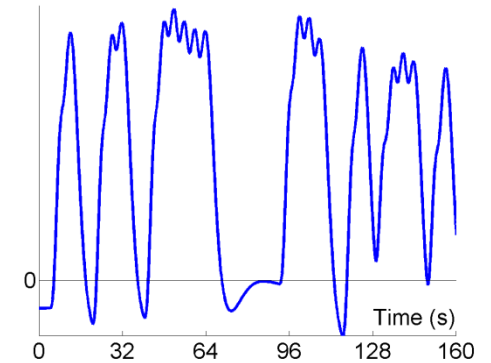
Stimulus ("Neural")



HRF

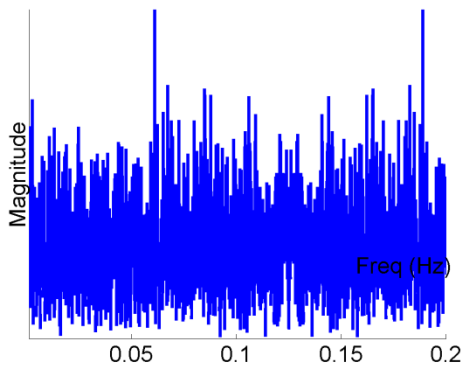


Predicted Data



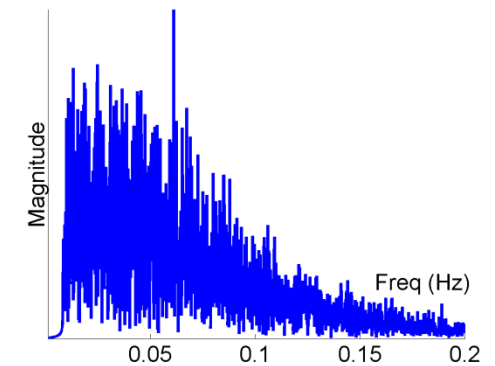
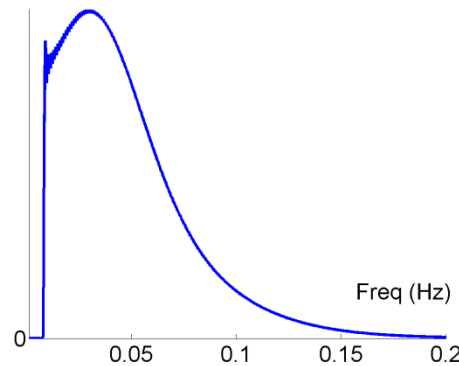
$\otimes$

=



$\times$

=



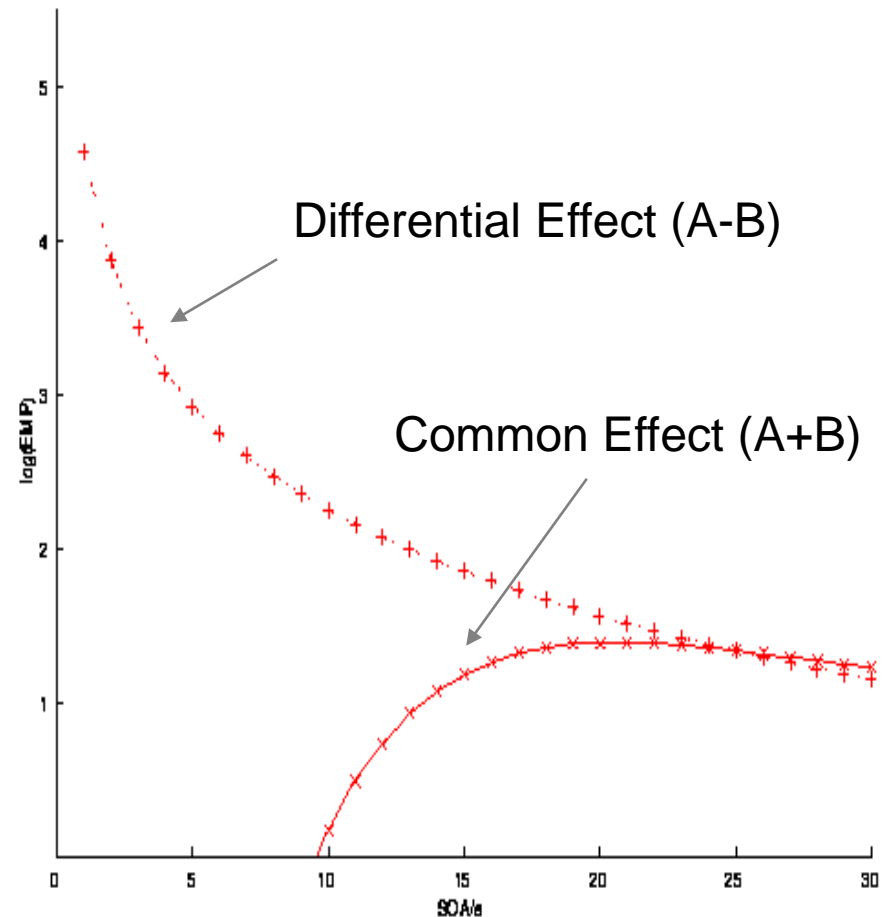
Randomised design spreads power over frequencies.

# Efficiency: Multiple event types

- Design parametrised by:  
 $SOA_{min}$  Minimum SOA  
 $p_i(\mathbf{h})$  Probability of event-type  $i$  given history  $\mathbf{h}$  of last  $m$  events
- With  $n$  event-types  $p_i(\mathbf{h})$  is a  $n^m \times n$  Transition Matrix
- Example: Randomised AB

	<b>A</b>	<b>B</b>
<b>A</b>	0.5	0.5
<b>B</b>	0.5	0.5

=> **ABBBABAABABAAA...**



4s smoothing; 1/60s highpass filtering

# Efficiency: Multiple event types

- Example: Alternating AB

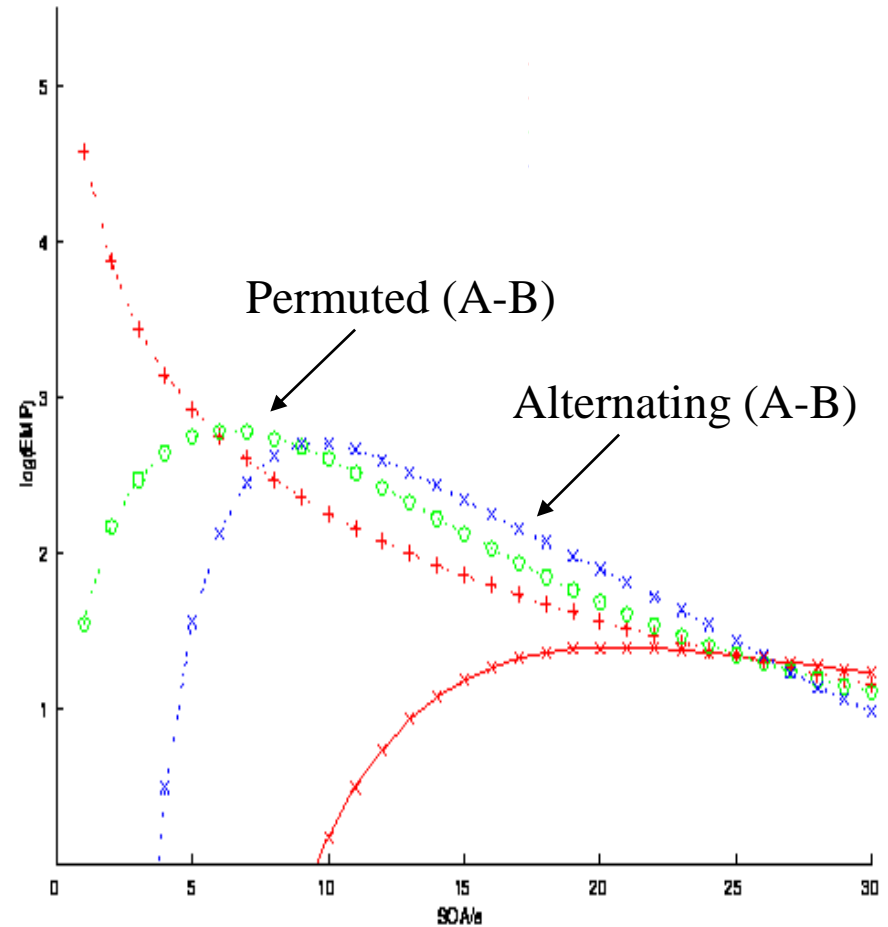
	<b>A</b>	<b>B</b>
<b>A</b>	0	1
<b>B</b>	1	0

=> **ABABABABABAB...**

- Example: Permuted AB

	<b>A</b>	<b>B</b>
<b>AA</b>	0	1
<b>AB</b>	0.5	0.5
<b>BA</b>	0.5	0.5
<b>BB</b>	1	0

=> **ABBAABABABBA...**



*4s smoothing; 1/60s highpass filtering*

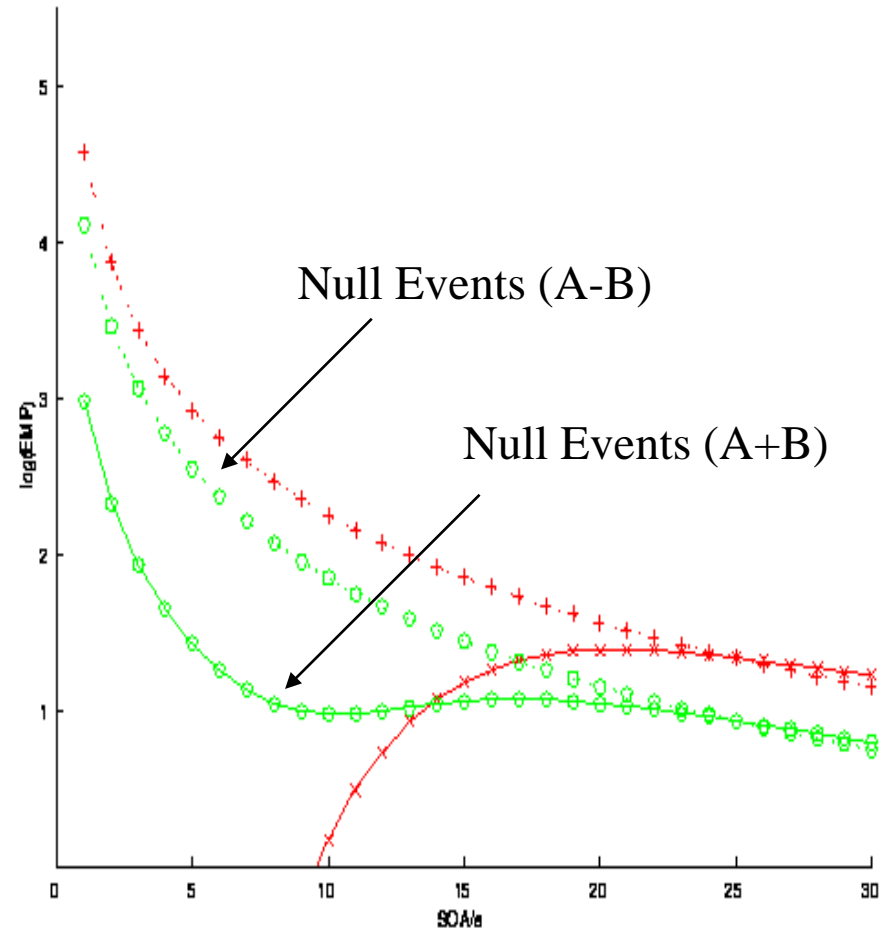
# Efficiency: Multiple event types

- Example: Null events

	<b>A</b>	<b>B</b>
<b>A</b>	0.33	0.33
<b>B</b>	0.33	0.33

=> **AB-BAA--B---ABB...**

- Efficient for differential *and* main effects at short SOA
- Equivalent to stochastic SOA (null event corresponds to a third unmodelled event-type)



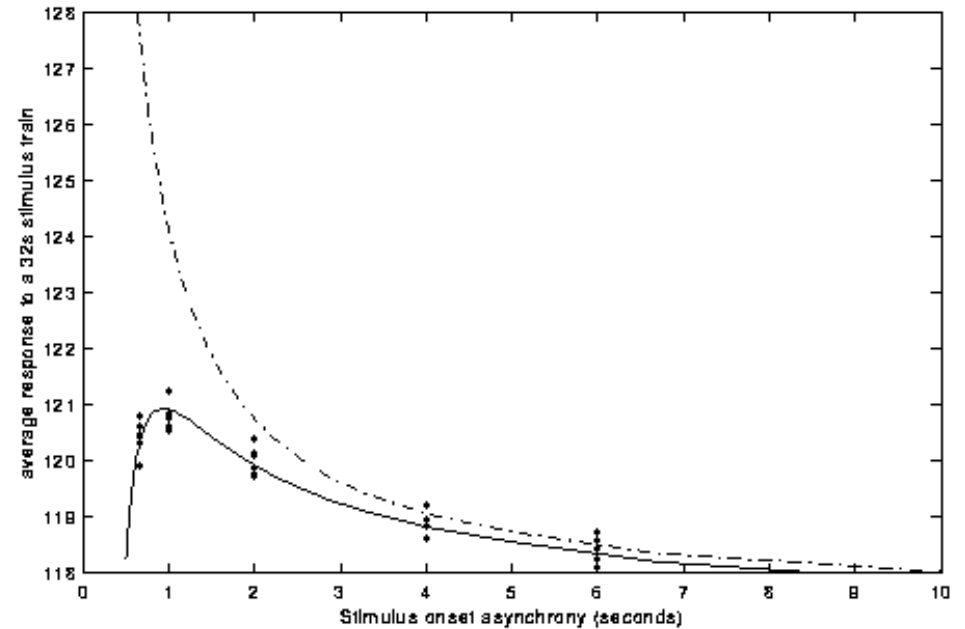
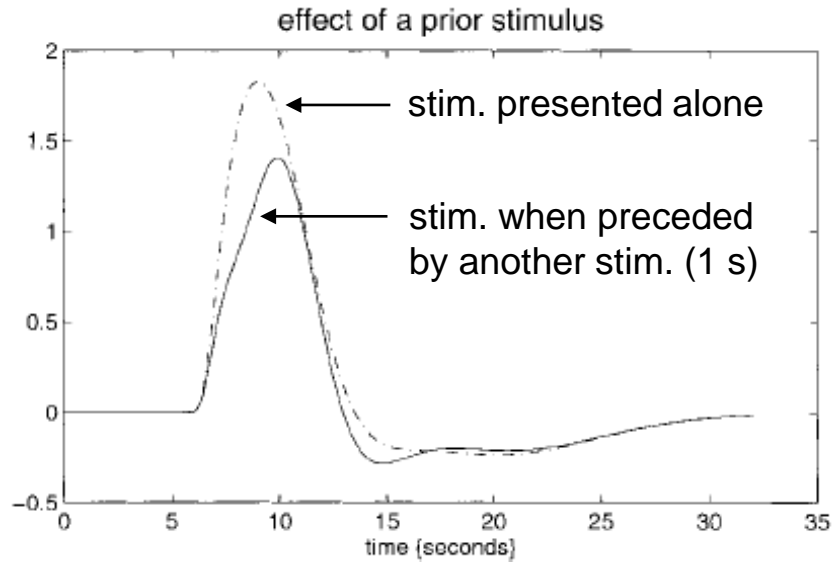
*4s smoothing; 1/60s highpass filtering*



# Design efficiency: Conclusions

- Optimal design for one contrast may not be optimal for another
- Blocked designs generally most efficient (with short SOAs, given optimal block length is not exceeded)
- However, psychological efficiency often dictates intermixed designs, and often also sets limits on SOAs
- With randomised designs, optimal SOA for differential effect (A-B) is minimal SOA (>2 seconds, and assuming no saturation), whereas optimal SOA for main effect (A+B) is 16-20s
- Inclusion of null events improves efficiency for main effect at short SOAs (at cost of efficiency for differential effects)
- If order constrained, intermediate SOAs (5-20s) can be optimal
- If SOA constrained, pseudorandomised designs can be optimal (but may introduce context-sensitivity)

# But beware: Nonlinearities at short SOAs



**Thank you**